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# Dynamic contrast-enhanced near-infrared spectroscopy using indocyanine green on moderate and severe traumatic brain injury: a prospective observational study

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**Background:** The care given to moderate and severe traumatic brain injury (TBI) patients may be hampered by the inability to tailor their treatments according to their neurological status. Contrast-enhanced near-infrared spectroscopy (NIRS) with indocyanine green (ICG) could be a suitable neuromonitoring tool.

**Methods:** Monitoring the effective attenuation coefficients (EAC), we compared the ICG kinetics between five TBI and five extracranial trauma patients, following a venous-injection of 5 mL of 1 mg/mL ICG, using two commercially available NIRS devices.

**Results:** A significantly slower passage of the dye through the brain of the TBI group was observed in two parameters related to the first ICG inflow into the brain ( $P=0.04$ ;  $P=0.01$ ). This is likely related to the reduction of cerebral perfusion following TBI. Significant changes in ICG optical properties minutes after injection ( $P=0.04$ ) were registered. The acquisition of valid optical data in a clinical environment was challenging.

**Conclusions:** Future research should analyze abnormalities in the ICG kinetic following brain trauma, test how these values can enhance care in TBI, and adapt the current optical devices to clinical settings. Also, studies on the pattern in changes of ICG optical properties after venous injection can improve the accuracy of the values detected.

**Keywords:** Near-infrared spectroscopy (NIRS); traumatic brain injury (TBI); indocyanine green (ICG); cerebral perfusion; blood-brain barrier (BBB)

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## Introduction

Over the last decade, the burden of global neurotrauma has been on the rise (1). The efficacy of the care given to these patients has been called into question: a randomized clinical trial to test hypothermia therapy was terminated early due to its poor outcomes (2); Cooper *et al.* reported that performing early decompressive craniectomies for the treatment of intracranial hypertension did not enhance patient outcomes (3), while Hutchinson *et al.* reported a lower mortality rate in patients who undertook ‘last resort’ decompressive craniectomies, but only modest improvement to outcomes (4). One of the main differences between the studies from Cooper *et al.* and the one from Hutchinson *et al.* is that, while in the former the decompressive craniectomy was performed as one of the first therapeutic interventions, in the latter it was one of the last, made following other unsuccessful interventions. This may lead one to think that only a portion of those who had been under surgery in the study of Cooper *et al.* would have found the decompressive craniectomy beneficial, while the others could have received a more conservative treatment.

Chesnut *et al.* suggested that the lack of subtype-classification in recruited TBI patients may be responsible for the limited improvements observed (5). This is linked fundamentally to limitations in injury burden stratification with current multimodal neuromonitoring tools (6): computed tomography (CT), for example, limits analysis to anatomical pathology without giving a clear picture of the complexity of post-injury pathophysiology (particularly at the bedside) including neuronal injury, perfusion deficiency, metabolic crisis, etc. (7,8). The intracranial pressure (ICP) has fundamental limitations in that it is only a surrogate for cerebral perfusion, calculated via the differential between the pressure in the systemic vasculature and in the head. The ICP monitor limits analysis to the brain area in which it is inserted and cannot record different effects of trauma across the hemispheres (9). This motivates the adoption of detectable biomarkers in clinical neurotrauma, and the importance of coupling them to radiological patterns including magnetic resonance imaging (MRI), or other objective biological measurements into more robust and reliable biosignatures (10).

Cerebral perfusion and the integrity of the blood-brain barrier (BBB) can be impaired after brain trauma (11,12). The analysis of these two parameters, either focally or globally, could comprise a more in-depth assessment of a patient’s status and provide an alternative method for

stratifying their severity. This can lead to:

- (I) Development of novel treatments to reverse the directly observed pathology;
- (II) Better direction of existing therapy towards individuals most likely to experience benefit.

Near-infrared spectroscopy (NIRS) can be a useful non-invasive, continuous, bedside neuromonitoring tool in the care of TBI patients (13). Studies on humans and animals have measured cerebral perfusion and vascular permeability after brain trauma by monitoring the kinetics of a contrast dye, indocyanine green (ICG), with NIRS devices (14-17). Unlike NIRS, other dynamic contrast-enhanced imaging techniques (i.e., CT, MRI) expose patients to ionizing radiation and/or cannot be performed continuously at the patients’ bedsides (18). Currently, the ICG cerebral vascular kinetics monitored through contrast-enhanced NIRS in TBI patients remains to be fully investigated clinically.

ICG is a contrast dye with absorption and fluorescence properties in the NIR spectral range, and is commonly used in clinical practice (e.g., neuro-oncology; theranostic nanomedicine) (19-22). The ICG photon absorption is related to the dye concentration and to the nature of the solvent in which it is dissolved (23). In water, an increase in dye concentration drives changes in its absorption coefficient due to the progressive formation of ICG aggregates, which have an absorption peak at 690 nm wavelength, starting from the ICG monomers, which have a peak at 785 nm (19,23,24). In blood, ICG is bound by a large spectrum of proteins and lipids (19,25). This binding process shifts the absorption peak to approximately 810 nm within a few seconds and stabilizes the dye’s optical properties by interfering with the formation of ICG aggregates (19,23,26).

Herein, we monitored the ICG kinetics in the brains of TBI and extracranial trauma (non-TBI) patients by measuring the effective attenuation coefficient (EAC) at multiple wavelengths, using two commercially available depth-resolved continuous-wave (CW) and frequency-domain (FD)-NIRS devices (27-30). During the first ICG passage into the cerebral circulation, we hypothesized that we would observe an ICG optical signal for a longer period of time in the TBI group than in the non-TBI group, due to more impaired and attenuated brain perfusion in the former than in the latter. We also anticipated a prolonged ICG signal in the TBI group within a few minutes post-injection, due to leakage of the dye into the interstitial tissue of the parenchyma as a result of increased BBB permeability.

Furthermore, we compared the ICG absorption



**Figure 1** Representation of the positions of the NIRO-200NX probes on a TBI patient's forehead in ITU. A scale shows the distance in centimeters between one of the two probes and the patient's nasion. TBI, traumatic brain injury; ITU, intensive therapy unit.

properties at different wavelengths after injection by analyzing the slow changes in the EAC. We hypothesized that the highest level of photon absorption by the ICG would be at around 810 nm, and no significant changes to ICG optical properties would be observed after a few seconds from the injections.

## Methods

### Equipment

A three wavelengths (735 nm, 810 nm, 850 nm) CW-NIRS device, NIRO-200NX (Hamamatsu Photonics, Tokyo, Japan), and a two-wavelengths (690 nm, 830 nm) FD-NIRS device, ISS-OxiplexTS™ (ISS Inc., Champaign, Illinois, USA) were used.

Both these devices employ a spatially resolved spectroscopy (SRS) NIRS approach with multiple source-detector distances (31,32). The SRS approach permits enhanced sensitivity to deep (few cm) structures and inference of the EAC, which is related to the exponential decay of the light signal with distance (27).

### Participants

Five moderate and severe TBI (three males; mean age: 58) and five non-TBI patients (three males; mean age: 59), admitted to the ward or the intensive therapy unit (ITU)

of the Queen Elizabeth Hospital Birmingham (UK) were enrolled into the study. Participants with suspected liver or kidney dysfunction were excluded from the study.

Four TBI patients were tested less than 14 days from injury (mean days: 8) while under sedation and one TBI patient, affected by chronic subdural hematoma, after more than three months while non-sedated. In all four acute TBI patients, the Glasgow Coma Scale (GCS) score at admission was 12 or lower, while in the other patient it was 15. All TBI patients had a CT scan with signs of brain trauma. Three TBI patients had an ICP monitor at the time of observation, two of them had an ICP lower than 20 mmHg and one patient had an ICP of 25 mmHg; one TBI patient passed away from the severity of injuries incurred acutely.

Non-TBI patients had GCS scores between 14 and 15 at admission; no signs of traumatic brain injury (TBI) were reported on the CT scan; non-TBI patients were all awake and orientated at the time of recording.

Two TBI and three non-TBI patients were scanned with the NIRO-200NX; three TBI and two non-TBI patients with the ISS-OxiplexTS™.

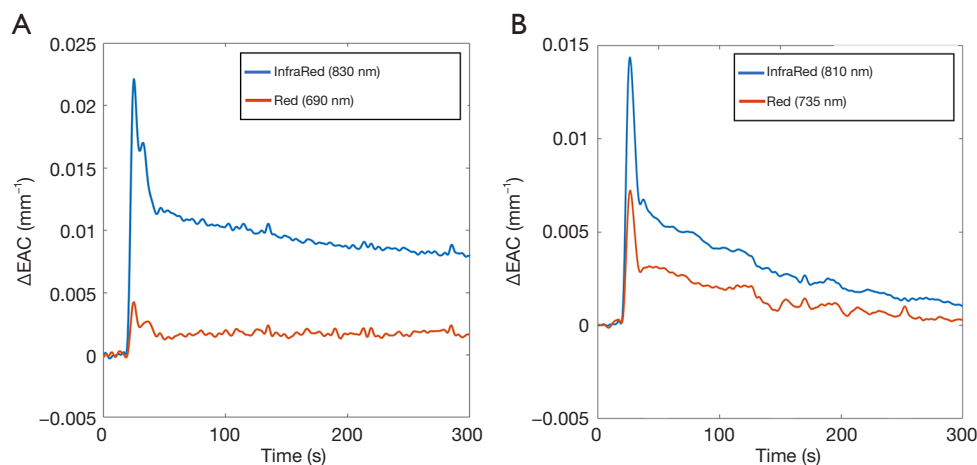
Initially, the data were acquired from 15 moderate and severe TBI (12 males; mean age: 30) and 12 non-TBI patients (8 males; mean age: 48). However, the analysis had to be reduced to the aforementioned five moderate or severe TBI and five non-TBI patients because of the low signal-to-noise ratio in the rest of the sample.

### Data acquisition

The study [Near Infra RED Cerebral Spectroscopy in the DIrection And early MONitoring of therapy in patients with traumatic brain injury (RED DIAMOND)] was approved by the East of England-Cambridge Central Research Ethics Board (Ref REC: 14/EE/0165; IRAS ID: 144979). Awake patients took part in this study after providing informed written consent. For those in an incapacitated state, a written consent form was received from the next of kin or from a person designated to give consent. The study conforms to the Declaration of Helsinki (as revised in 2013).

The optical probes were positioned on the patients' foreheads to monitor each hemisphere (*Figure 1*). The channels' positions were consistent across participants. If the signal was oversaturated, a bandage or a black sheet was applied on top of the probes to reduce ambient light. Awake participants were instructed to stay as still as they could.

An ICG powder for injection of 25 mg, Verdyne



**Figure 2** Examples of changes to the EAC evaluated with the (A) FD-NIRS ISS-OxiplexTSTM and the (B) CW-NIRS, NIRO-200NX. EAC, effective attenuation coefficient.

(Diagnostic Green GmbH, Aschheim, Germany), was mixed with 25 mL of water for injection. From this solution, two boluses of 5 mL of 1 mg/mL ICG were injected into the patients' venous peripheral cannulae or central lines. Following each injection, 5 mL of saline for injection was immediately flushed into the same cannula.

The optical signal was recorded for 2 and 10 minutes, respectively, before and after each ICG injection.

### NIRS data analysis

#### ICG's kinetic

The ICG passage through the brain was assessed by evaluating the changes to EAC based on the CW light attenuation with distance (Figure 2) (27).

The phase shift registered by the FD-NIRS ISS-OxiplexTS<sup>TM</sup> was ignored.

The EAC (expressed in  $\text{mm}^{-1}$ ) is proportional to the geometric mean of the absorption and reduced scattering coefficients of the volume investigated (33). Since the reduced scattering coefficient can be considered constant during the ICG dynamic, changes to EAC were considered directly related to the effect of the ICG absorption.

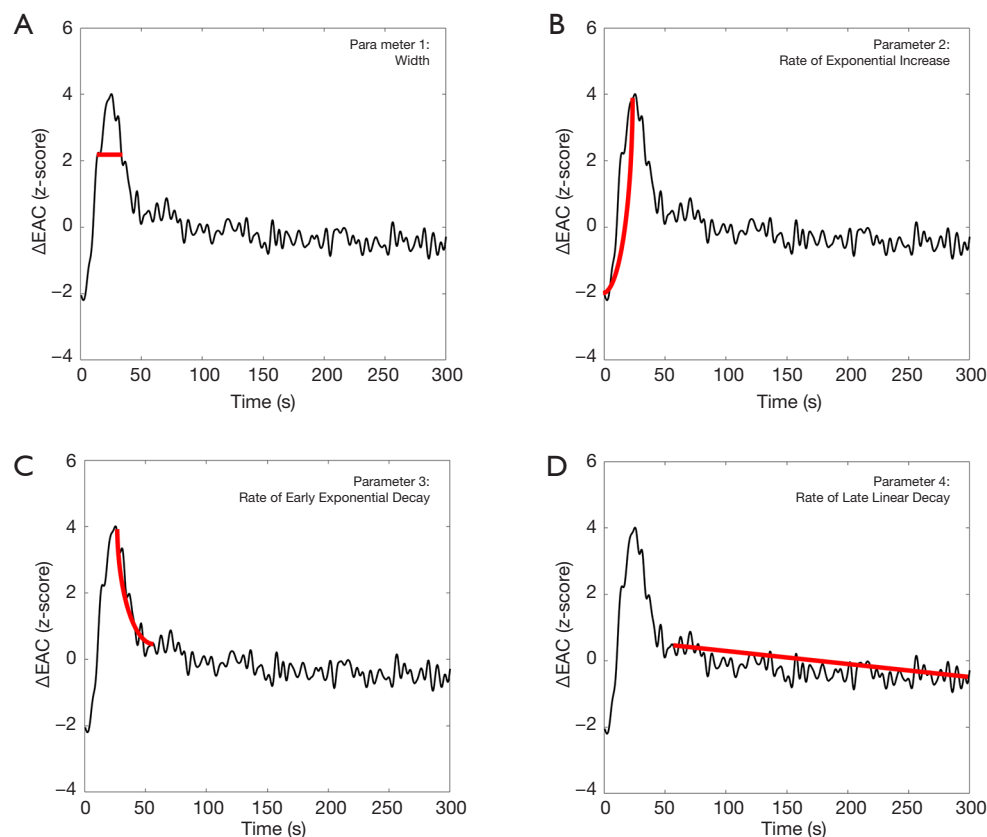
The EAC measured by the CW-NIRS and the FD-NIRS devices were combined: given their similar wavelengths, the changes to EAC at the wavelengths 735 and 690 nm (red) and the changes at 810 and 830 nm (infrared) were merged together.

In order to compare the EAC temporal dynamics among different subjects, the EAC curves were normalized

(z-scored), and several parameters were evaluated. A first parameter to be evaluated was the *width* of the EAC curve. This width was estimated at 30% of the maximum EAC value (expressed in s, Figure 3A). Moreover, the EAC temporal dynamic was divided into three temporal ranges characterized by an *early exponential increase*, an *early exponential decay*, and a *late linear decay* (Figure 3B,C,D). The parameters associated with these three temporal ranges were two exponential rates of increase (positive value) and decay (negative value) and one rate of linear decay (negative value), all expressed in  $\text{s}^{-1}$ . The *late linear decay* was considered for up to 5 minutes from injection due to the low ICG signal-to-noise ratio beyond this. The four extracted curve parameters were separately compared between the TBI and non-TBI groups using Student's *t*-test.

Similar to other contrast-enhanced imaging techniques (e.g., CT, MRI), the *early exponential decay*, the *late linear decay* and the *width* of the first passage of the dye bolus are indicative of cerebral perfusion; the *early exponential decay* was related to the ICG washing out which can be delayed if the ICG passed from the vascular space, where it was physiologically confined, to the interstitial brain tissue following BBB damage (18,34). A translation of the ICG optical signal on TBI patients into absolute parameters of cerebral blood flow (CBF) and BBB may be inaccurate and unnecessary to answer the current clinical needs (14). As a result, the analysis of the ICG kinetic was limited to the differences in ICG optical signal between the TBI and non-TBI groups, without resolving this into CBF or BBB values.





**Figure 3** Example of a normalized (z-scored) EAC dynamic following ICG injection. Four parameters were extracted from each EAC curve: (A) width; (B) rate of early exponential increase; (C) rate of early exponential decay; and (D) rate of late linear decay. EAC, effective attenuation coefficient; ICG, indocyanine green.

### ICG's optical properties

During the *late linear decay*, changes in the z-score of EAC in the TBI and non-TBI groups were merged together and the *late linear decay* between the red and the infrared were compared using the paired sample *t*-test. As mentioned in Sec. ICG's kinetic, changes of EAC were considered directly related to the ICG absorption properties changes.

## Results

### ICG's kinetics

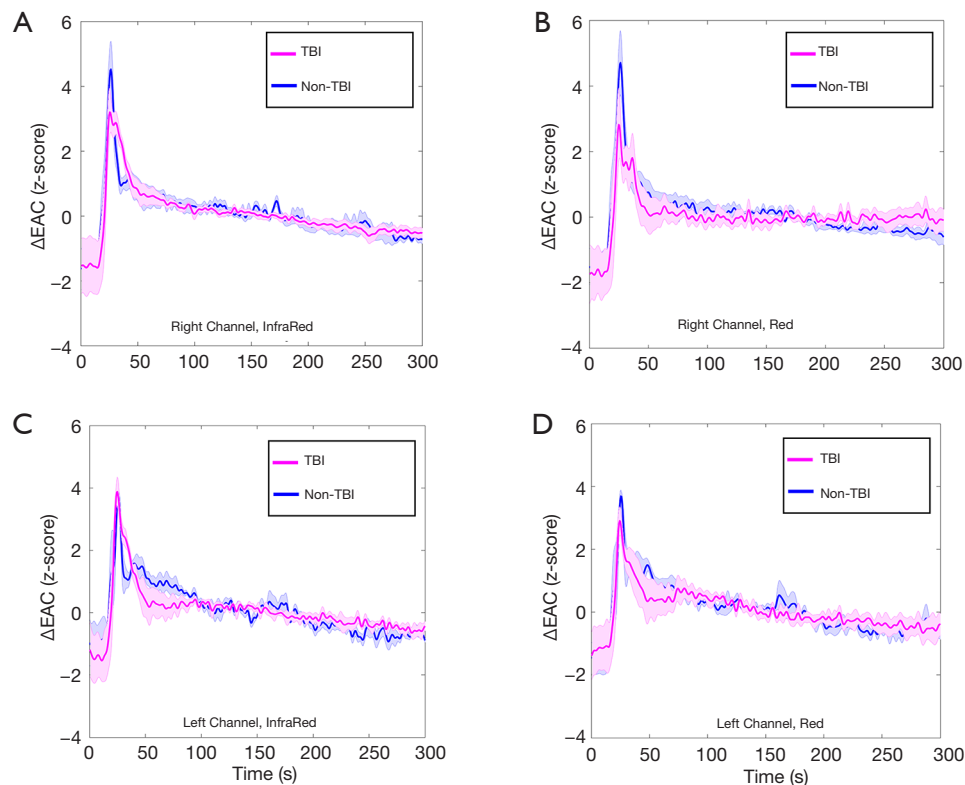
Figure 4 shows averaged and normalized EAC temporal dynamics of TBI and non-TBI patients for different combinations of channel locations (left and right) and wavelengths (red and infrared).

The standard error of the mean is also reported. Clear differences between TBI and non-TBI ICG temporal

dynamics are visible.

Figure 5 displays box-and-whisker plots of the various parameters for different combinations of channel locations (left and right), wavelengths (red and infrared) and groups (TBI and non-TBI patients).

Significant statistical differences between TBI and non-TBI patients ( $P < 0.05$ ) were obtained for the width parameter of the infrared signal in the right channel (*t*-score: 2.34, *df*=8,  $P=0.04$ ) and for the early exponential decay parameter of the InfraRed signal in the right channel (*t*-score: 3.12, *df*=8,  $P=0.01$ ). Although not statistically significant, a similar trend for the width (larger for TBI patients) and the rate of early exponential decay (smaller in absolute value for TBI patients) parameters were found for all combinations of channels and colors. On the contrary, the rate of exponential increase and rate of late linear decay did not show any significant differences between the two groups considered.



**Figure 4** Average of the normalized (z-scored) EAC curves in TBI and non-TBI patients. (A) Right channel, infrared light; (B) right channel, red light; (C) left channel, infrared light; and (D) left channel, red light. EAC, effective attenuation coefficient; TBI, traumatic brain injury.

### ICG's optical properties

In order to evaluate possible changes with time in the ICG optical properties, statistical comparisons (Student's paired t-tests) between the EAC curve parameters at each wavelength were performed. Interestingly, the *rate of late linear decay* was the only parameter showing statistically significant differences between red and infrared (t-score: 2.38, df=9, P=0.04). Considering the temporal characteristics and the negative values of the *rate of late linear decay*, the result depicts a stronger increase in the attenuation in the InfraRed, probably associated with a slow modification to the ICG optical properties.

## Discussion

### ICG's kinetics

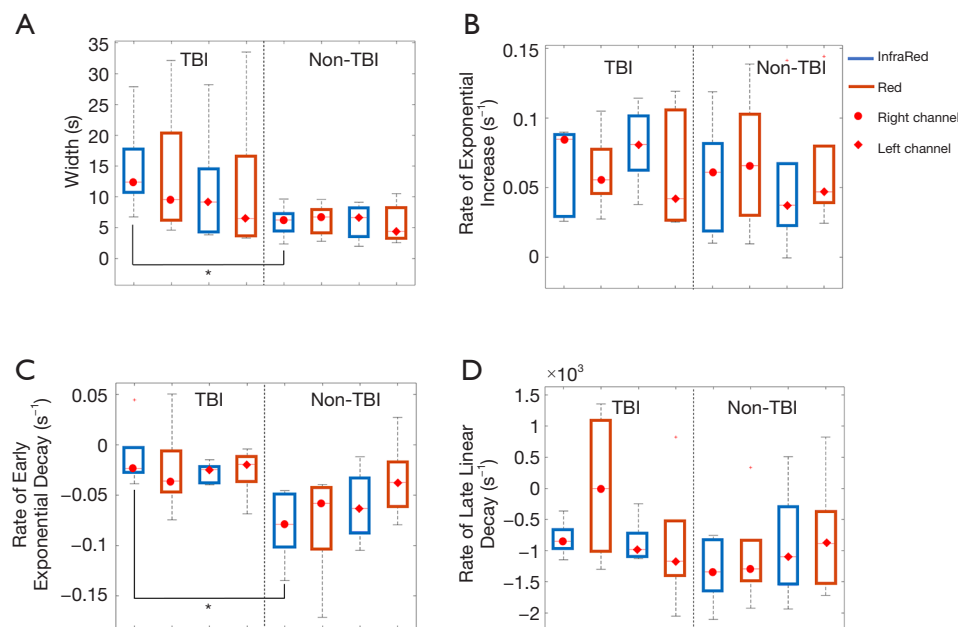
#### First ICG's passage

During the first ICG passage, in the right channels for the InfraRed color, the *width* and the *early exponential decay* of

the EAC curve were significantly different between TBI and non-TBI patients. This can be related to reduced cerebral perfusion in the TBI group than in the non-TBI one, which slows the movement of the ICG bolus through the brain in the former as opposed to the latter. This result agrees with the literature where a broader curve of bolus passage due to vascular impairment is reported (35).

Similar trends in the *width* and *early exponential decay* were also seen in the left channels, however, the difference between TBI and non-TBI patients was not significant. The cerebral perfusion in TBI patients is inhomogeneous across the brain, therefore the different grades of *width* and *early exponential decay* between right and left channels could be the result of different grades of abnormal perfusion between hemispheres after a brain injury.

In both channels, there was no significant difference in the *initial increase* between the TBI and non-TBI groups. Previous studies in brain trauma and stroke patients reported changes of diffuse reflectance due to a delayed dye inflow related to vascular impairments (15,35–38).



**Figure 5** Box-and-whisker plots of the different parameters for different combinations of channel locations (left and right), wavelengths (red and infrared) and groups (TBI and non-TBI patients). The EAC curve parameters evaluated were (A) width; (B) rate of exponential increase; (C) rate of early exponential decay; and (D) rate of late linear decay. EAC, effective attenuation coefficient; TBI, traumatic brain injury.

However, there was no evidence of a similar delay in this study. The disagreement between the results herein exposed and those reported by previous studies can be related to the different optical analyses performed. In those aforementioned studies, the delay of ICG inflow was assessed through a comparison between intracranial (ICT) and extracranial tissues (ECT) or between hemispheres in the same patient. This was possible either because the vascular lesion of stroke patients could be identified in a specific hemisphere, or because the use of a time-domain (TD)-NIRS allowed for the separation of the ECT and ICT signals by plotting the distribution of time of flight of photons (DToF). These two analyses were not possible in this study: in TBI patients a comparison between affected and non-affected hemispheres cannot easily be performed as the reduction of cerebral perfusion often affects different parts of the brain inconsistently; the optical analysis performed herein facilitated the relation of changes in optical signal according to depth, but not the separation of inflow into the ECT and the ICT as can be done using DToF. It should be noted that, in agreement with our results, a direct comparison of values of *initial increase* between patients with vascular impairments and controls did not show a significant difference (37).

### ICG's retention

Although, in both channels, the *late linear decay* was not significantly different between TBI and non-TBI patients, in the right channel, the trend suggests a higher level of photon absorption by ICG in the TBI group than in the non-TBI one.

In the minutes which followed the first ICG bolus passage, the continuous decrease of ICG concentration in the illuminated volume is related to the dilution of dye within the blood compartment and its uptake by the liver (20,39). This process can be delayed in areas with BBB damage due to dye leakage into the interstitial tissue. In such a scenario, the dye outflows from the vascular system until its concentration in the vessels is lower than that in the interstitial tissue (34). These kinetics explain the higher concentration of the dye measured in the right channel of the TBI patients. The lack of statistical significance of the *late linear decay* in the right channels between the TBI and non-TBI groups may be related to the small sample size considered.

It should also be noted that the BBB damage may be present in some brain areas only and the ICG leakage would thus be limited to these areas alone (40). Therefore, some TBI patients may not have had BBB damage in



their right hemisphere and so did not show a higher ICG concentration, with consequences for the statistical difference between the groups. Similarly, the different levels of EAC between right and left channels may be due to the inhomogeneity of BBB damage across the injured brain, which itself may have been present in the right rather than the left hemisphere in the TBI population examined.

### Extracranial trauma patients as controls

A comparison between trauma patients could increase the accuracy of the analysis of brain abnormalities through ICG kinetics. To our knowledge, this is the first study that has analyzed ICG kinetics in the brain of TBI patients using patients who suffered extracranial trauma as controls.

After a trauma, liver perfusion can be reduced with consequences for ICG clearance (41,42). Hence, a comparison between healthy subjects and TBI patients may mistake hepatic perfusion abnormalities for alterations in the brain, or the former can influence the values of the latter.

Furthermore, there can be a systemic inflammatory response following a trauma (43). As highlighted regarding liver perfusion abnormalities, a comparison between TBI and non-TBI patients helps to reduce the effects that an inflammatory response can have on the results obtained.

### ICG's optical properties

During the *late linear decay*, there was a significant increase of ICG photon absorption at the InfraRed light compared to that at the Red light. This is in agreement with the changes in ICG absorption peak following binding with plasma components and explains why ICG kinetics could have been monitored using InfraRed rather than Red wavelengths (19,23).

However, contrary to our hypothesis, there was no spectral stabilization a few seconds post-injection as the changes of ICG optical properties continued throughout the *late linear decay*. The longer time for ICG spectral stabilization to occur could be related to the need for the bolus to disperse into the bloodstream. This explanation is partially in agreement with a previous study that showed changes of optical density *in vivo* after 20–35 seconds from the ICG injection, due to the dye-blood intermixing process (44). It should also be noted that in that study, the authors calculated the ICG optical properties retrospectively at the beginning of the recording based on the spectrum of absorption once the dye was intermixed with blood (44).

The time of spectral stabilization may also have been prolonged by the formation of ICG aggregates while the ICG was dissolved in a water solution before it was injected. This is because the ICG aggregates cannot directly bind to plasma compounds, but they are progressively disaggregated into monomers by the binding process (23). The percentage of ICG aggregates, and so the time of spectral stabilization, would vary between patients because the time that the ICG stays in a pre-injection water solution is not constant. Furthermore, the different percentages of ICG aggregates between patients would affect the extent of any changes to ICG optical properties during the spectral stabilization, as ICG aggregates and monomers have different absorption peaks.

The small sample size considered in this study does not allow for an in-depth analysis of the changes in optical properties across individuals. However, considering the prolonged time for spectral stabilization to occur during *in vivo* experiments, future studies should investigate the variables connected to the changes of ICG absorption spectrum, as this may affect the accuracy of the kinetic analysis and measurements of the ICG concentration. Inaccuracies in the values of ICG concentration could be particularly relevant when the ICG concentration is used to retrieve absolute values of CBF and BBB damage (14). In addition, these results suggest that even if the dye kinetics can be mainly monitored using InfraRed wavelengths at approximately 810 nm, analysis at multiple wavelengths should be preferred during *in vivo* experiments in order to track the changes of dye optical properties.

### Limitations

#### Signal-to-noise ratio

A low signal-to-noise ratio may completely obscure the *initial increase* and the *early exponential decay* and severely compromise the *late linear decay* of an EAC curve. As a consequence, the quality of the recording related to that injection would be irreversibly affected.

The initial group of 15 TBI and 12 non-TBI patients had to be reduced to five TBI and five controls because of poor signal-to-noise ratios. This can be explained by the difficulties in acquiring data in challenging clinical environments due to multiple elements (e.g., illuminated environment, ecchymosis on the scalp, mechanical constraints) or the difficulties in clinicians using commercially available NIRS devices. In its current state, this level of quality control exclusion would not allow for direct translation of this technique into clinical practice.

### Merged signal from different wavelengths

The diffuse reflectance obtained at different wavelengths (810, 830, and 690, 735 nm, respectively) was merged together. This can be considered an approximation and may have interfered with the accuracy of the results.

### Fluorescence signal

The fluorescence signal emitted by the ICG was not considered in this study.

Steinkellner *et al.* highlighted that in a system based on the level of dye photon absorption, its fluorescence signal should be considered as contamination (35). However, using a TD-NIRS device with and without fluorescence blocking filters, they reported a negligible effect of the fluorescence signal on the total number of photons, which can be considered as the optical signal measured in the study herein presented (35).

### Sedation

Four of the TBI patients were sedated at the time of the measurement, while none of the controls were under sedation. The drugs used to sedate the TBI patients (e.g., propofol, midazolam) have a hypoperfusion effect on the CBF (7,45). The different cerebral perfusion measured between the two groups could be partially explained by the effect of these drugs in the sedated patients. It should be noted that the different results between right and left channels suggests that the reduction of cerebral perfusion cannot be limited to the effects of the sedation alone.

### Comparison of the optical parameters measured with biomarkers of brain trauma

The aims of this study were limited to the differences in optical signal between TBI and non-TBI patients, and no analysis was carried out to investigate correlation between the optical abnormalities detected and other TBI biomarkers (e.g. hyperglycemia) (46).

Future multimodal monitoring studies should investigate how optical abnormalities are linked with other TBI biomarkers in order to better understand the pathogenetic mechanism responsible for these abnormalities and to include the optical results in TBI biosignatures for clinical practice (10,47).

### Conclusions

To conclude, using contrast-enhanced NIRS, we registered differing ICG kinetics between a TBI and a non-TBI group

of patients. This difference can be related to abnormalities of cerebral perfusion and vascular permeability following a brain injury. Future larger studies should better quantify the changes in ICG kinetic after brain injury and test the efficacy of these values to enhance the treatments of TBI patients.

We also report difficulties in collecting high-quality optical data in clinical settings. This calls into question the viability of current commercially available NIRS devices for contrast-enhanced neuromonitoring for clinical purposes. Future work should aim to enhance the user-friendliness of these optical devices for applications of contrast-enhanced NIRS in clinical settings, similar to what has been done in other optical techniques (48,49).

Contrary to our hypothesis, changes in ICG optical properties were seen for minutes after injection. Future research should aim to better define the pattern of changes of ICG optical properties during *in vivo* experiments to enhance the accuracy of contrast-enhanced NIRS with ICG.

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### Footnote

**Conflicts of Interest:** All authors have completed the ICMJE uniform disclosure form (available at <http://dx.doi.org/10.21037/qims-20-742>). The authors report grants from European Union Horizon 2020 Research and Innovation Program, and from Polish National Science

Centre, during the conduct of the study.

**Ethical Statement:** The study conforms to the Declaration of Helsinki (as revised in 2013) and was approved by East of England-Cambridge Central Research Ethics Board (Ref REC: 14/EE/0165; IRAS ID: 144979) and informed consent was taken from all the patients. Written informed consent was obtained from the patient for publication of this study and any accompanying images. A copy of the written consent is available for review by the Editor-in-Chief of this journal.

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